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(54) Title: POLYMERIC CARRIERS FOR RELEASE OF COVALENTLY LINKED AGENTS

(57) Abstract

A chemically defined polymeric carrier comprising a series of α -amino acids in any combination containing side chains to which diagnostic/therapeutic and chelating agents can be covalently joined through cleavable linkers either directly or covalently joined through cleavable linkers after chemical modification of the side chains. Hydrazone, disulfide, and ester linkages in any combination can be present in the polymeric carrier between the side chains of the α -amino acids and the agents. The presence of a particular covalent linkage between the side chain and the agent in the carrier is determined by the functional group present in the side chain of the α -amino acid and the functional group present in the agent. The α -amino acids with side chains to which agents do not covalently join can function as spacers to minimize interaction between bulky molecules attached to the polymeric carrier. In addition, those α -amino acids with charge or hydrophilic side chains to which agents do not covalently join can provide increased solubility to the polymeric carrier.

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POLYMERIC CARRIERS FOR RELEASE OF COVALENTLY LINKED AGENTS

BACKGROUND OF THE INVENTION

1. Field of the Invention

5 The invention relates to chemically defined polymeric carriers that provide advantageous properties for in vivo imaging and therapy. The polymeric carriers consist of α -amino acids that contain side chains covalently joined to (i) diagnostic and therapeutic molecules and (ii)
10 chelating agents capable of binding diagnostic or therapeutic radionuclides.

2. Related art

15 Monoclonal antibodies have been developed that localize in cancerous tissue, due to their high specificity and affinity for antigens on tumor cell surfaces. This development has increased the prospect of clinical applications, if such antibodies can be linked to
20 diagnostic and therapeutic agents. The high specificity of the antibodies makes them desirable candidates as targeting molecules for delivering a diagnostic or therapeutic agent to a cancer site.

25 Unfortunately, the direct linkage of such agents to an antibody weakens its immunoreactivity. Any derivatization of the antibody weakens its immunoreactivity. Therefore, an antibody with multiple linkages to diagnostic or therapeutic agents is an antibody with low specificity. At the present time, chelating agents, which
30 bind to diagnostic and therapeutic radionuclides, are

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directly linked to antibodies. This precludes the controlled release of the radionuclide from the antibodies. Due to the large size of the antibody molecule, it is difficult, using conventional detection techniques, to determine the exact nature of the chelating agent linkages to the antibody, and to determine the number of chelating agents linked to the antibody. A lack of such precise information presents problems for getting regulatory approval of chelating agents. Regulatory agencies require that all substances subject to their approval must include information that clearly identifies the structure of the substance, which is to be introduced into the body.

What is needed is an approach that derivatizes a targeting molecule, such as an antibody, at a minimum number of sites to carry larger amounts of diagnostic and therapeutic agents. Also needed, is an approach that can determine the nature of the chelating agent linkage to the antibody and the number of chelating agents linked to the antibody.

SUMMARY OF THE INVENTION

5 The present invention provides a chemically defined
polymeric carrier. It comprises a series of α -amino
acids, in any combination, containing side chains to which
diagnostic/therapeutic and chelating agents can be
covalently joined through cleavable linkers. The agents
can be covalently joined to the side chains through
10 cleavable linkers either directly or covalently joined to
the side chains through cleavable linkers after chemical
modification of the side chains. Hydrazone, disulfide, and
ester linkages, in any combination, can be present in the
polymeric carrier between the side chains of the α -amino
15 acids and the agents. The selection of a particular
covalent linkage between the side chain and the agent in
the polymeric carrier is determined by the functional
group in the α -amino acid side chain and the reactive
functional group in the agent. The α -amino acids with side
20 chains to which agents do not covalently join can function
as spacers, to minimize interaction between the bulky
molecules attached to the polymeric carrier. In addition,
those α -amino acids with charged or hydrophilic side
chains to which agents do not covalently join can provide
25 increased solubility to the polymeric carrier.

N-terminal protecting groups which are optional for the
polymeric carrier include all the standard amine
protecting groups. C-terminal conjugation groups which
30 are optional for attachment of the polymeric carrier to
the targeting molecule include all conjugation groups
known in the art. In order to provide efficient
attachment of the polymeric targeting molecule, a spacer

- 4 -

group is present in the polymeric carrier between the α -amino acids and the conjugation group. The spacer group presents any steric hindrance to the attachment by any agent appended from the C-terminal end of the carrier.

5 These spacer groups are terminal aminoacids, such as γ -aminobutyric acid (Aba). In the absence of the conjugation group, the spacer group, e.g., Aba through its carboxyl group, can attach the polymeric carrier to the targeting molecule.

10 The peptides that constitute the polymeric carrier are prepared from α -amino acids by conventional solution methods or by solid-phase peptide synthesis. These peptides have been modified to carry derivatized

15 diagnostic/ therapeutic agents, and chelating agents that bind to diagnostic and therapeutic radionuclides. These agents can be released either at the target site or after internalization by the cell.

20 Many advantages arise from the present invention. The polymeric carrier can carry a maximum number of agents while derivatizing a targeting molecule at a minimum number of sites. Thus the biological activity of the targeting molecule is maintained at a high level, even

25 though it is attached to multiple agents. For example, the fewer the linkages in an antibody, the higher is its specificity.

30 The rate at which agents can be released from the polymeric carrier attached to the targeting molecule is controlled by manipulating the nature of the covalent linkages in the polymeric carrier. For example, by adjusting the stability of the covalent linkages or by

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using different types of covalent linkages on a polymeric carrier, agents--are released at a mixed rate. This is particularly important when the disease requires use of long term diagnostics or therapeutics.

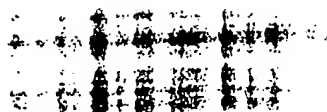
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Multiple agents, which may be the same or different, are attached to the polymeric carrier. Not only can the same agents be released at a mixed rate, but different agents can be released at a mixed rate in the same target site.

10

The polymeric carrier, with its covalently linked agents, is a relatively small molecule compared to the targeting molecule. Therefore, conventional detection techniques can predetermine the exact nature of the agent linkages to the targeting molecule before the polymeric carrier is attached to it. In addition, radiolabeling techniques can determine the precise number of polymeric carriers linked to the targeting molecule.

15



BRIEF DESCRIPTION OF THE FIGURES

5 Figure 1 is a flow chart representing the general procedure for synthesis of a polymeric carrier with attached agents and the conjugation of the polymeric carrier to an antibody.

10 Figure 2 is a flow chart representing a procedure for the synthesis of a polymeric carrier with attached therapeutic agents and the conjugation of the polymeric carrier to an antibody.

15 Figure 3 illustrates the removal of protecting groups from amino acid side chains of a polymeric carrier.

20 Figures 4 and 6 are flow charts representing procedures for the synthesis of polymeric carriers with attached chelating agents and the conjugation of the polymeric carriers to antibodies.

 Figure 5 is a flow chart representing a procedure for the synthesis of a chelating agent.

DETAILED DESCRIPTION OF THE INVENTION

The present invention relates to a chemically defined polymeric carrier that increases the loading of diagnostic/therapeutic and chelating agents to targeting molecules. The polymeric carrier comprises a series of from 2 to about 18 α -amino acids in any combination that include side chains which can covalently join through cleavable linkers to agents. The number of agents covalently joined through cleavable linkers to the polymeric carrier can be from 2 to about 18. This number is determined by the number of α -amino acid side chains in the polymeric carrier available for covalent bonding through cleavable linkers to the agents.

The term "polymeric carrier" as used in the invention denotes a peptide carrier. Those α -amino acids whose side chains are not covalently joined to agents can function as spacers for the polymeric carrier. These spacers reduce any non-bonded interactions between agents attached to modified α -amino acids. In addition to acting as spacers, those α -amino acids with charged or hydrophilic side chains not covalently joined to agents can impart increased solubility to the polymeric carrier.

The polymeric carrier includes optionally a protecting group at its N-terminal end and optionally a conjugation group at its C-terminal end. The conjugation group enables the polymeric carrier to attach itself to a targeting molecule. A spacer group is placed between the α -amino acids and the conjugation group to aid in the attachment of the polymeric carrier to the targeting molecule. The spacer group prevents any steric hindrance to the

attachment by any agent appended from the C-terminal end of the carrier. In addition, the spacer group, a terminal amino acid, may attach the polymeric carrier to the targeting molecule without the presence of the conjugation group. This may occur by reacting the carboxyl group of the terminal amino acid with functional groups on the targeting molecule to form covalent bonds, such as ester and amide linkages.

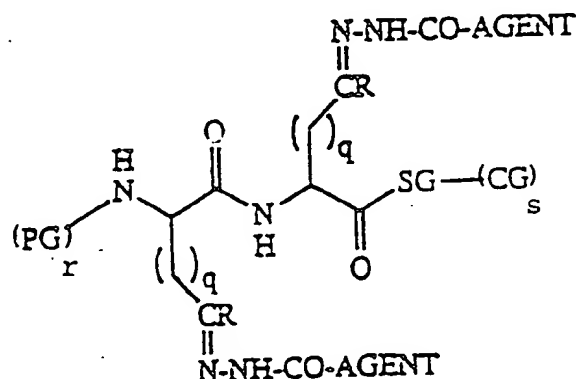
In the polymeric carrier, α -amino acids having side chains that enhance polarity and therefore, water solubility, are desirable. The increased water solubility is believed to further contribute to decreased hepatobiliary uptake of radiolabeled polymeric carrier proteins. The α -amino acids having side chains that enhance water solubility include those with charged side chains (lysine, arginine, histidine, cysteine, aspartic acid, glutamic acid, tyrosine, tyrosine-O-SO₃⁻) and those with hydrophilic side chains (serine, threonine, asparagine, glutamine). Standard amine protecting groups can be used for the N-terminal protecting group of the polymeric carrier. Preferred embodiments of the invention comprise acetyl, propionyl, phenylacysulfonyl, substituted phenylacysulfonyl, and other hydrophilic protecting groups.

A conjugation group is a chemically reactive functional group that will react with a targeting molecule to bind the polymeric carrier thereto. When the targeting molecule is a protein, the conjugation group is reactive under conditions that do not denature or otherwise adversely affect the protein. Therefore, the conjugation group is sufficiently reactive with a functional group on

a protein so that the reaction can be conducted in a substantially aqueous solution and does not have to be forced, e.g., by heating to high temperatures, which may denature the protein. Examples of suitable conjugation groups include but are not limited to active esters, isothiocyanates, amines, hydrazines, maleimides or other Michael-type acceptors, thiols, and activated halides. Among the preferred active esters are N-hydroxysuccinimidyl ester, sulfosuccinimidyl ester, thiophenyl ester, 2,3,5,6-tetrafluorophenyl ester, and 2,3,5,6-tetrafluorothiophenyl ester. The latter three preferred active esters may comprise a group that enhances water solubility, at the para (i.e., 4) or the ortho position on the phenyl ring. Examples of such groups are CO_2H , SO_3^- , PO_3^{2-} , OPO_3^{2-} , OSO_3^- , N^+R_3 wherein each R represents H or an alkyl group, and $\text{O}(\text{CH}_2\text{CH}_2\text{O})_n\text{CH}_3$ groups.

Terminal amino acids used as spacer groups in the invention include aminocaproic acid, aminopentanoic acid, γ -aminobutyric acid, β -alanine, glycine, and the like.

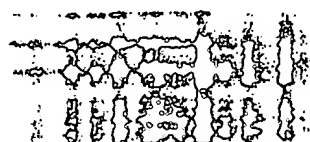
Agents containing hydrazides, $\text{R}(\text{CO})\text{NHNH}_2$, react with α -amino acid side chains containing aldehydes, RCHO , or ketones, $\text{R}_2(\text{CO})$, to form polymeric carriers with hydrazone linkages having the following formula:



- 10 -

5 wherein the α -amino acids in the polymeric carrier are
from 2 to about 18 units;
PG is an N-terminal protecting group;
SG is a spacer group that by preventing steric
hindrance by agents appended from the C-
10 terminal end of the carrier promotes efficient
attachment of the polymeric carrier to a
targeting molecule;
CG is a conjugation group useful for the
attachment of the polymeric carrier to a
15 targeting molecule;
AGENT is from 2 to about 18 units of a
diagnostic or therapeutic agent, or a chelating
agent capable of binding diagnostic or
therapeutic radionuclides in the polymeric
20 carrier;
R is H, CH₃, phenyl, or phenyl substituted with
electron-donating and/or electron-withdrawing
groups;
q is 0 or 1;
25 r is 0 or 1; and
s is 0 or 1.

Hydrazone formation is an effective method of attaching
certain therapeutic agents to monoclonal antibodies (King
et al., Biochemistry, Vol. 25:5774, 1986). Recent work in
30 the area of therapeutic immunoconjugates addressed the
hydrazone functionality as a potentially cleavable linker
between a chemotherapeutic agent and a monoclonal
antibody. Laguzza et al., (J. Med. Chem., Vol. 32:548,
1989) demonstrated that a vinca alkaloid can be conjugated
35 to an antibody via a hydrazone linkage and that pH



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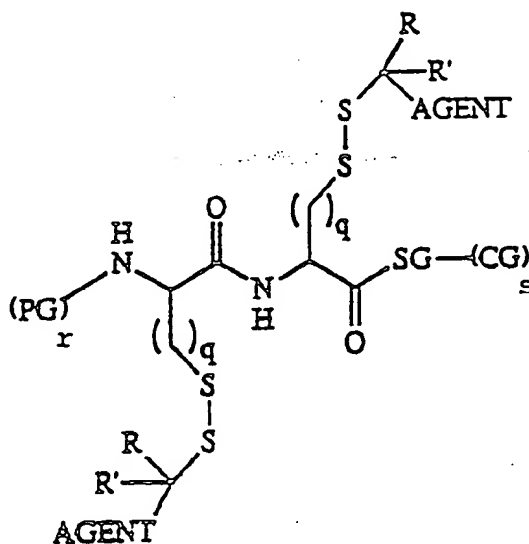
dependency of the drug could be studied. The hydrazone linkage approach was based on the premise that a conjugate formed via a serum stable, yet acid-labile hydrazone linker would serve the purpose of delivering the drug conjugate to the tumor site and then slowly release upon exposure to the tumor's acidic environment (Tannock et al., Cancer Research, Vol. 49:4373, 1989). This conditional requirement necessitated the screening of several small molecule hydrazones to evaluate their stability in human serum and acetate buffer at pH 5.6.

The design of the polymeric carrier system with a hydrazone linkage incorporates the observed results of a small molecule study. Peptides of known amino acid sequences are constructed to carry primary or secondary hydroxyl groups (the chain may carry more than one hydroxy amino acid (primary or secondary), which can be oxidized to the carbonyl compound.

The results of the small molecule study indicate that hydrazones from aromatic aldehydes may be too stable to be useful. Hydrazones derived from aliphatic ketones have a serum half-life of 15-20 hours (generated in the peptides from threonine and other aminoacids containing secondary -OH groups). Hydrazones derived from aliphatic aldehydes (generated in the peptides from serine, homoserine and other amino acids containing primary -OH groups) have a serum half-life of 50-60 hours. Hydrazones derived from aromatic ketones (generated in the peptides from phenylserine and substituted phenylserines)) have a serum half-life of 130 hours. By choosing an antibody or its fragment with a half-life in human serum similar to that of hydrazone, maximum delivery of the antibody or its

fragment to the tumor is expected. After which, the release of the therapeutic unit could occur at a rate dependent on the chosen hydrazone's half-life in the tumor site's acidic environment. To prevent the polymeric carrier from possible premature degradation, the polymeric carrier can be constructed with only D-amino acids or a mixture of D- and L-amino acids.

Agents containing thiols, SH, react with cysteine side chains to form polymeric carriers with disulfide linkages having the following formula:



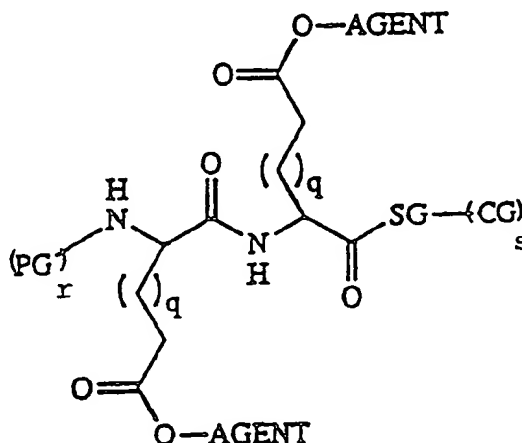
- 13 -

5 wherein the α -amino acids in the polymeric carrier are
 from 2 to about 18 units;
 PG is an N-terminal protecting group;
 SG is a spacer group that by preventing steric
 hindrance by agents appended from the C-
10 terminal end of the carrier promotes efficient
 attachment of the polymeric carrier to a
 targeting molecule;
 CG is a conjugation group useful for the
 attachment of the polymeric carrier to a
15 targeting molecule;

 AGENT is from 2 to about 18 units of a
 diagnostic or therapeutic agent, or a chelating
 agent capable of binding diagnostic or
20 therapeutic radionuclides in the polymeric
 carrier;
 R is H or CH_3 ;
 R' is H or CH_3 ; and
 q is 1 or 2;
25 r is 0 or 1; and
 s is 0 or 1.

30 The release rate for agents linked through disulfide bonds
 to the polymeric carrier can be decreased by replacement
 of hydrogen with α -alkyl groups ($\text{R}, \text{R}' = \text{CH}_3$).

Agents containing hydroxyl groups react with aspartic and glutamic acid side chains to form polymeric carriers with ester linkages having the following formula:



wherein the α -amino acids in the polymeric carrier 2 to about 18 units;

20

PG is an N-terminal protecting group;

SG is a spacer group that by preventing steric hindrance by agents appended from the C-terminal end of the carrier promotes efficient attachment of the polymeric carrier to a

25

targeting molecule;

CG is a conjugation group useful for attachment of the polymeric carrier to a targeting molecule;

30

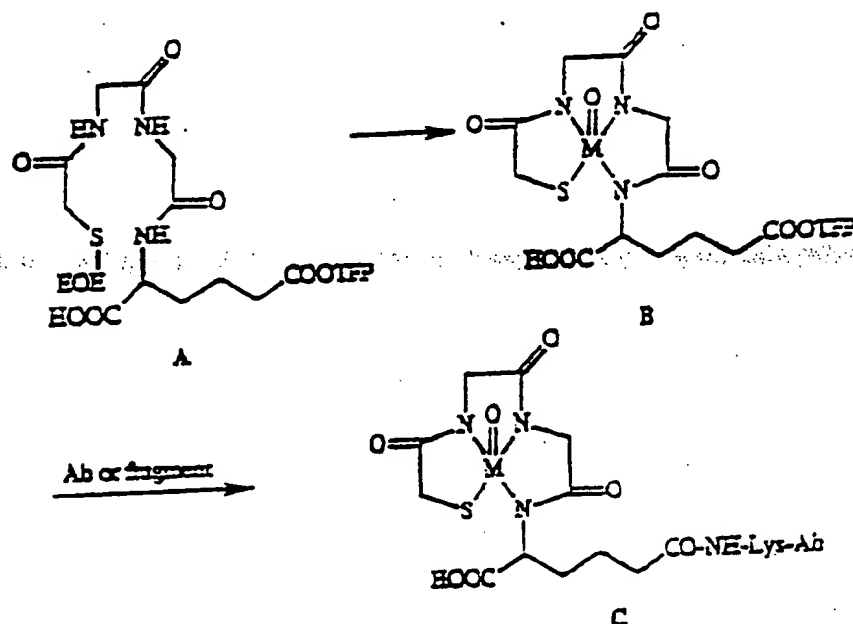
AGENT is from 2 to about 18 units of a diagnostic or therapeutic agent, or a chelating agent capable of binding diagnostic the or therapeutic radionuclides in the polymeric carrier;

q is 0 or 1;

r is 0 or 1; and

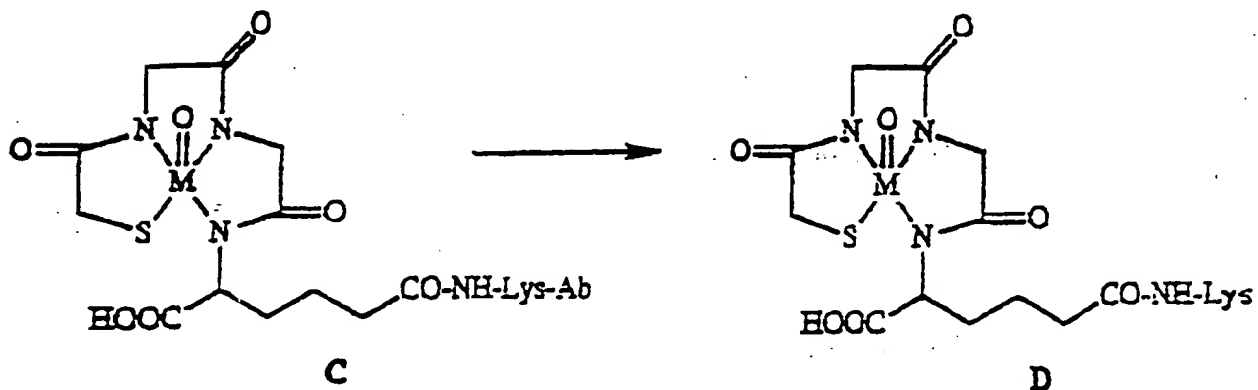
s is 0 or 1.

In general, attachment of radionuclide metals (e.g., M = ^{99m}Tc , ^{186}Re or ^{188}Re) to monoclonal antibodies using bifunctional chelating agent A has been carried out by the following procedure. Formation of M-chelate containing active ester B followed by attachment to monoclonal antibodies to give C, according to the following reaction scheme:

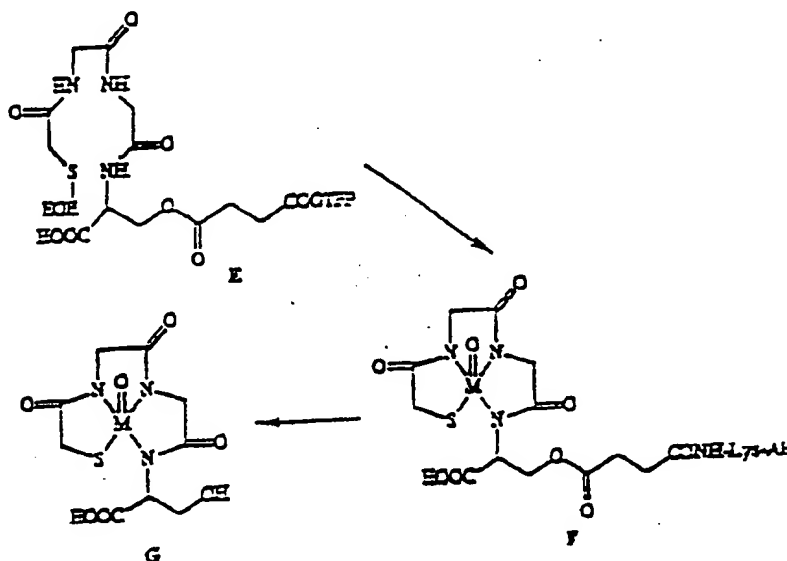


EOE refers to an ethoxy ethyl protecting group. COOTFP refers to 2,3,5,6-tetrafluorophenyl ester. The above chelate is an N_3S derivative, and N_2S_2 derivatives follow a similar procedure. Between the chelate and the antibody

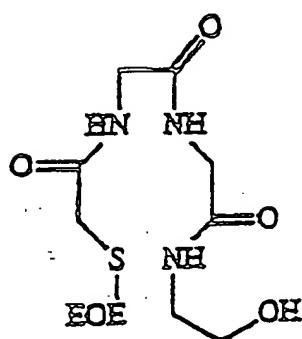
is a carbon chain attached to the α -amino group of the antibody. After metabolism takes place in various organs, the major metabolite D is retained in the gut and kidney and is not excreted, according to the following:



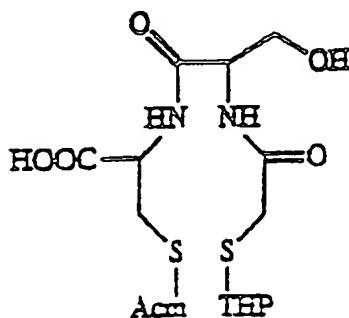
5 This retention interferes with imaging in the lower
abdominal area and gives a high dose to the kidney during
therapy. It was found that the presence of a cleavable
linker between the chelate and the antibody (compound F,
10 prepared from E) is metabolized and results in the
formation of G, which has no retention in the gut and low
retention in the kidney, according to the following
reaction scheme:



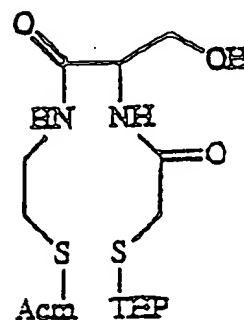
- 5 The observation that the cleavable linker is metabolized in the above reaction scheme leads to attaching the hydroxy groups of the following compounds:



H



J



K

to the aspartic and glutamic acid side chains to form ester linkages in the polymeric carriers.

20

The resulting polymeric carrier can carry more than one radionuclide metal/per attachment to the antibody or fragment and offers the advantage of a metabolite that can be removed via the renal system instead of being retained in the gut.

25

Compound H belongs to N_3S type chelates and J and K belong to the N_2S_2 chelate system. The groups THP (tetrahydropyranyl) and AcM (acetamidomethyl) are used as sulfur protecting groups.

30

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The targeting molecule is any molecule that will serve to deliver the polymeric carrier with attached diagnostic/therapeutic or chelating agents to a desired target site (e.g., target cells) in vitro or in vivo.

5 Examples of targeting molecules include, but are not limited to, steroids, cholesterol, lymphokines, and those drugs and proteins that bind to a desired target site.

10 The targeting molecule may be a targeting protein, which is capable of binding to a desired target site. The term "protein" as used herein includes proteins, polypeptides, and fragments thereof. The targeting protein may bind to a receptor, substrate, antigenic determinant, or other binding site on a target cell or other target site. The
15 targeting protein serves to deliver the agent attached thereto by polymeric carrier to a desired target site in vivo. Examples of targeting proteins include, but are not limited to, antibodies and antibody fragments, hormones, fibrinolytic enzymes, and biologic response modifiers. In
20 addition, other molecules that localize in a desired target site in vivo although not strictly proteins, are included within the definition of the term "targeting proteins" as used herein. For example, certain carbohydrates or glycoproteins may be used in the present
25 invention. The proteins may be modified, e.g., to produce variants and fragments thereof, as long as the desired biological property (i.e., the ability to bind to the target site) is retained. The proteins may be modified by using various genetic engineering or protein engineering
30 techniques.

Among the preferred targeting proteins are antibodies, most preferably monoclonal antibodies. A number of

- 20 -

monoclonal antibodies that bind to a specific type of cell have been developed including monoclonal antibodies specific for tumor-associated antigens in humans. Among the many such monoclonal antibodies that may be used are anti-TAC, or other interleukin-2 receptor antibodies; 9.2.27 and NR-ML-05, reactive with the 250 kilodalton human melanoma-associated proteoglycan; and NR-LU-10, reactive with a pancarcinoma glycoprotein. The antibody employed in the present invention may be an intact (whole) molecule, a fragment thereof, or a functional equivalent thereof. Examples of antibody fragments are $F(ab')_2$, -Fab', Fab, and F_v fragments, which may be produced by conventional methods or by genetic or protein engineering.

Proteins contain a variety of functional groups; e.g., carboxylic acid (COOH) or free amine ($-NH_2$) groups, which are available for reaction with a suitable protein conjugation group on a polymeric carrier to bind the polymeric carrier to the targeting protein. For example, an active ester on the polymeric carrier reacts with epsilon amine groups on lysine residues of proteins to form amide bonds. Alternatively, a targeting molecule and/or a polymeric carrier may be derivatized to expose or attach additional reactive functional groups. The derivatization may involve attachment of any of a number of linker molecules such as those available from Pierce Chemical Company, Rockford, Illinois. (See the Pierce 1986-87 General Catalog, pages 313-54.) Alternatively, the derivatization may involve chemical treatment of the protein (which may be an antibody). Procedures for generation of free sulfhydryl groups on antibodies or antibody fragments are also known. (See U.S Patent No.

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4,659,839). Maleimide conjugation groups on polymeric carriers are reactive with the sulfhydryl (thiol) groups.

5 Alternatively, when the targeting molecule is a carbohydrate or glycoprotein, derivatization may involve chemical treatment of the carbohydrate; e.g., glycol cleavage of the sugar moiety of a glycoprotein antibody with periodate to generate free aldehyde groups. The free
10 aldehyde groups on the antibody may be reacted with free amine or hydrazine conjugation groups on polymeric carriers.

In the present invention, therapeutic agents (e.g., a drug, therapeutic radionuclide or toxin) are attached to
15 the chemically defined polymeric carrier. Preferably, multiple therapeutic agents (which may be the same or different) are attached to the polymeric carrier. Exemplary therapeutic agents include toxins and drugs. Within the present invention, preferred toxins include
20 holotoxins, such as abrin, ricin, modecin, Pseudomonas exotoxin A; Diphtheria toxin, pertussis toxin and Shiga toxin; and A chain or "A chain-like" molecules, such as ricin A, abrin A chain, modeccin A chain, the enzymatic portion of pertussis toxin, the enzymatic portion of Shiga
25 toxin, gelonin, pokeweed antiviral protein, saporin, barley toxin, and snake venom peptides.

Exemplary drugs include daunomycin, adriamycin, vinblastine, doxorubicin, bleomycin, methotrexate,
30 5-fluorouracil, 6-thioguanine, cytarabine, cyclophosphamide, and similar conventional chemotherapeutics (for example, see Cancer: Principles and Practices of Oncology, 2d ed., V.T. DeVita, Jr., S.

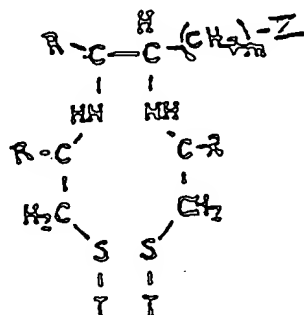
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Hellman, S.A. Rosenberg, J.B. Lippincott Co., Philadelphia, PA, 1985, Chapter 14). Yet other preferred drugs that can be used with the present invention belong to the tricothecene family, with Roridin A particularly preferred. Experimental drugs may also be suitable for used within the present invention (see, e.g., NCI Investigational Drugs Pharmaceutical Data 1987, NIH Publication No. 882141, Revised November 1987).

In the present invention, radiolabeled molecules are attached to the chemically defined polymeric carrier. Preferably, a multiple number of radiolabeled molecules (which may be the same or different) are attached to the polymeric carrier.

Radionuclide metal chelates are one type of radiolabeled molecule that may be employed. Many chelating compounds of various structures, as well as methods for the synthesis and radiolabeling thereof to produce radionuclide metal chelates, are known. Chelating compounds comprising various combinations of sulfur, nitrogen, oxygen, and phosphorous donor atoms may be used, for example. The chelating compound may, for example, comprise a total of from four to six donor atoms selected from nitrogen and sulfur atoms. During the radiolabeling procedure, bonds form between the donor atoms and the radionuclide metal, thereby producing a radionuclide metal chelate. Chelating compound(s) may be incorporated into the polymeric carrier during the synthesis procedure. Alternatively, the chelating compound(s) may be synthesized separately and subsequently attached to the polymeric carrier.

One type of chelating compound that may be employed comprises two nitrogen and two sulfur donor atoms and thus may be designated an "N₂S₂" chelating compound. Suitable N₂S₂ chelating compounds are described in U.S. Patent number 4,897,255, entitled "Metal Radionuclide Labeled Proteins for Diagnosis and Therapy", which is hereby incorporated by reference in its entirety. One example of an N₂S₂ chelating compound is as follows:

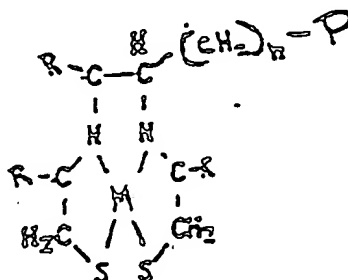


wherein n is from 1 to about 4 (preferably 2); each R independently is selected from =O and H₂; T represents a sulfur protecting group; and Z represents an active ester or other reactive functional group (which in the present invention may be useful for incorporating the chelating compound into the polymeric carrier).

Any suitable conventional sulfur protecting group(s) may be attached to the sulfur donor atoms of the compounds of the present invention. The protecting groups should be removable, either prior to or during the radiolabeling reaction. Among the preferred sulfur protecting groups are AcM and hemithioacetal protecting groups (EOE, THP), which

are displaceable from the chelating compound during the radiolabeling reaction.

5 The N_2S_2 chelating compound advantageously is radiolabeled after attachment to the polymeric carrier to produce a radionuclide metal chelate of the formula:



20 wherein P represents the polymeric carrier, M represents a radionuclide metal or oxide thereof, and the other symbols are as described above.

25 Radionuclide metals include, but are not limited to, the diagnostically effective radionuclide ^{99m}Tc , and the therapeutically effective radionuclides ^{188}Re , ^{186}Re , ^{67}Cu , ^{64}Cu , ^{212}Pb , ^{212}Bi , and ^{109}Pd . ^{186}Re and ^{188}Re are radionuclide metals for use in the present invention.

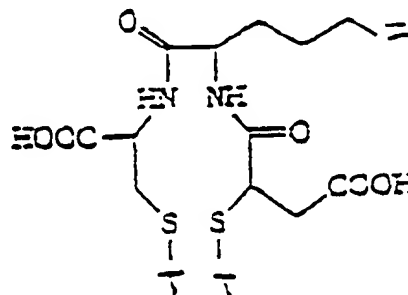
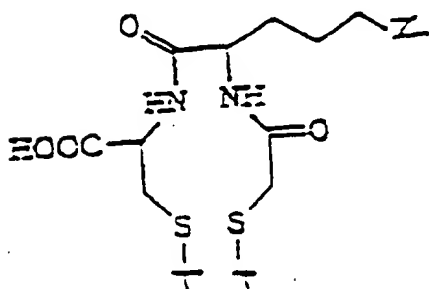
30 Methods for preparing these isotopes are known. Molybdenum/technetium generators for producing ^{99m}Tc are commercially available. Procedures for producing ^{186}Re include the procedures described by Deutsch et al., (Nucl.

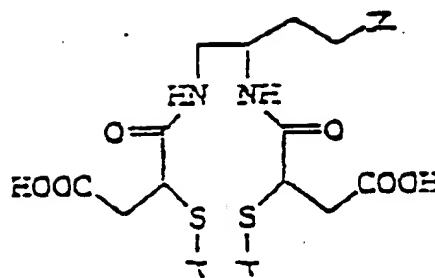
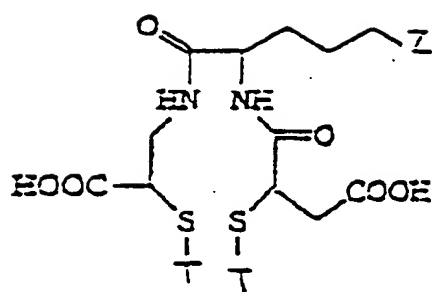
5 Med. Biol., Vol. 13:4:465-477, 1986) and Vanderheyden et al., (Inorganic Chemistry, Vol. 24:1666-1673, 1985), and ^{222}Bi methods for production of ^{188}Re have been described by Blachot et al. (Intl. J. of Applied Radiation and
10 Isotopes, Vol. 20:467-470, 1969) and by Klofutar et al. (J. of Radioanalytical Chem., Vol. 5:3-10, 1970). Production of ^{109}Pd is described in Fawwaz et al., J. Nucl. Med. (1984), 25:796. Production of ^{212}Pb and ^{222}Bi is described in Gansow et al., Amer. Chem. Soc. Symp. Ser. (1984), 241:215-217, and Kozah et al., Proc. Nat'l. Acad. Sci. USA (January 1986) 83:474-478.

15 The radiolabeling reaction (for this N_2S_2 compound and the other chelating compounds described below) is conducted using conventional procedures.

20 Additional N_2S_2 chelating compounds comprising carboxylic acid substituent(s) for improved biodistribution properties are described in copending U.S. Patent Application Serial number 07/367,502, entitled "Radionuclide Metal Chelates for the Radiolabeling of Proteins", which is hereby incorporated by reference.

Examples of such chelating compounds are as follows:

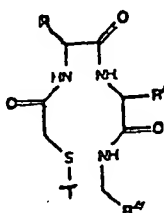




wherein the symbols T and Z are as described above for the
other N_2S_2 chelating compounds.

Another type of chelating compound that may be employed
comprises one sulfur and three nitrogen donor atoms and
thus may be designated an " N_3S " chelating compound
Suitable N_3S chelating compounds include those described
in European patent application publication number 284,071
and copending U.S. Patent Application Serial number

07/172,004, both entitled "Metal-Radionuclide-Labeled Proteins and Glycoproteins for Diagnosis and Therapy", which are hereby incorporated by reference in their entirety. Examples of N_3S chelating compounds include but are not limited to the following seven compounds, wherein "T" represents a sulfur protecting group and "COOTFP" represents a 2,3,5,6-tetrafluorophenyl ester group:



	R	R'	R''
Compound 1	H	H	$CH_2-CH_2-COOTFP$
Compound 2	CH_2-COOH	H	$CH_2-CH_2-COOTFP$
Compound 3	CH_2-COOH	CH_2-COOH	$CH_2-CH_2-COOTFP$
Compound 4	CH_2-CH_2-COOH	CH_2-COOH	$CH_2-CH_2-COOTFP$
Compound 5	H	$CH_2-CH_2-COOTFP$	$COOH$
Compound 6	$CH_2-CH_2-CH_2-COOTFP$	H	$COOH$
Compound 7	H	H	$CH_2-CH_2-COOTFP$

The COOTFP active ester may be replaced by other chemically reactive functional groups.

Other chelating compounds may have different combinations of donor atoms. Such compounds include among others, the N_2S_4 , N_2S_3 , and N_3S_3 chelating compounds described in copending U.S. Patent Application Serial no. 07/201,134, entitled "Metal Radionuclide Chelating Compounds for Improved Chelation Kinetics", which is hereby incorporated by reference in its entirety. In addition, the N_2S_2 and N_3S

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compounds presented above may comprise varying numbers of substituents such as carboxylic acid groups and from 0 to 3 oxygen atoms (=O) attached to carbon atoms of the chelate core.

5

In the present invention, the chelating compounds comprise, or are attached to, cleavable linkers. A number of linkers that are cleavable under defined conditions (e.g., at acidic pH, under reducing conditions, or in the presence of an enzyme such as a protease) are known. The chelates therefore may be released from the polymeric carrier under the desired conditions.

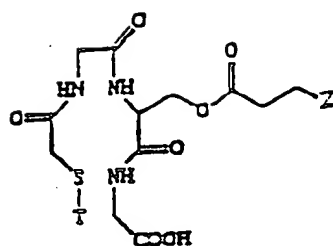
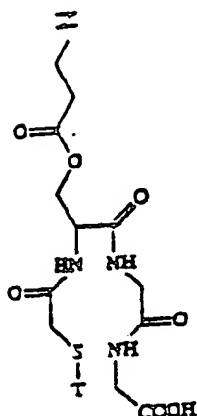
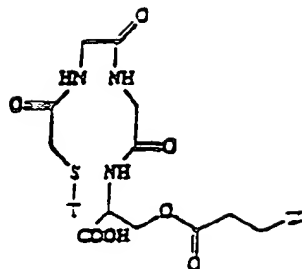
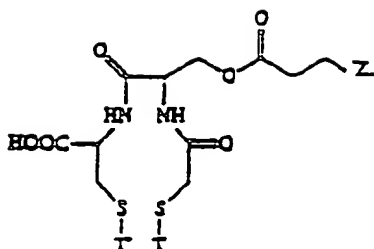
10

Suitable chelating compounds comprising a cleavable linkage include but are not limited to those described in copending U.S. Patent Application Serial no. 07/457,480, entitled "Radiolabeled Proteins for Diagnostic and Therapeutic Use", which is hereby incorporated by reference in its entirety. The U.S.S.N. 07/457,480 application discloses N_2S_2 and N_3S chelating compounds comprising a linker of defined structure that terminates in a chemically reactive functional group. The linkage is cleavable at an ester group positioned in a particular orientation therein. Examples of such chelating compounds include, but are not limited to, the following:

20

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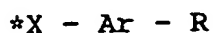




25 wherein T represents a sulfur protecting group and Z represents a chemically reactive group (e.g., an active ester) which may be used to incorporate the chelating compound into the polymeric carrier in accordance with the present invention.

30 Other examples of radiolabeled molecules that may be attached to the polymeric carrier in accordance with the present invention include radiohalogenated molecules. Examples of molecules that bind radiohalogens at the meta or para position on a phenyl ring are described in U.S. Patent No. 4,855,153, entitled "Radiohalogenated

Proteins", which is hereby incorporated by reference in its entirety. These compounds may be represented by the following formula:



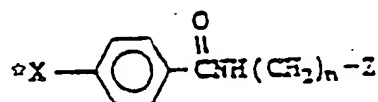
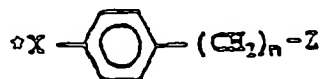
5 wherein

*X is a radioisotope of iodine, bromine, fluorine, or astatine;

Ar is an aromatic or heteroaromatic ring; and

10 R is a chemical bond or a substituent containing 1 to 12 straight-chain carbon atoms that does not activate Ar toward electrophilic substitution on the order produced by hydroxy or amino substitution of the ring. The bond or substituent has attached thereto a chemically reactive functional group useful in the present invention for incorporation of the compound (or a non-radiolabeled precursor thereof) onto the polymeric carrier.

15 *I-paraiodophenyl compounds (in which *I represents a radioisotope of iodine) may be prepared using procedures that generally involve substituting the organometallic group $Sn(n-Bu)_3$ or $SnMe_3$ on a haloaromatic compound. A radioisotope of a halogen then is substituted for the organometallic group by halodemetalization. Examples of
20 radiohalogenated molecules that may be prepared using such a procedure are represented by the following formulas:



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5 wherein n represents an integer from 0 to 3, Z represents a reactive functional group, and *X represents a radioisotope of a halogen.

10 Additional radiohalogenated molecules that may be used in the present invention are described in U.S. Patent No. 4,876,081, which is hereby incorporated by reference in its entirety. The radiohalogenated molecules comprise a vinyl group.

15 The radiolabeled polymeric carrier targeting molecules of the present invention have use in diagnostic and therapeutic procedures, both for in vitro assays and for in vivo medical procedures. The radiolabeled polymeric carrier molecules may be administered intravenously, 20 intraperitoneally, intralymphatically, locally, or by other suitable means, depending on such factors as the type of target site. The amount to be administered will vary according to such factors as the type of radionuclide (e.g., whether it is a diagnostic or therapeutic 25 radionuclide), the route of administration, the type of target site(s), the affinity of the targeting molecule for the target site of interest, and any cross-reactivity of the targeting molecule with normal tissues.

30 Appropriate dosages may be established by conventional procedures and a physician skilled in the field to which this invention pertains will be able to determine a suitable dosage for a patient. A diagnostically effective dose is generally from about 5 to about 35 mCi and typically from about 10 to about 30 mCi per 70 kg body 35 weight. A therapeutically effective dose is generally from about 20 mCi to about 300 mCi. For diagnosis,

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conventional non-invasive procedures (e.g., gamma cameras) are used to detect the biodistribution of the diagnostic radionuclide, thereby determining the presence or absence of the target sites of interest (e.g., tumors).

5

To render the ester in the polymeric carrier molecules of the present invention more susceptible to cleavage in the kidneys, an agent that raises urine pH may also be administered to the patient. Such agents include, for example, a salt of ascorbate (e.g., sodium ascorbate) or a bicarbonate salt (e.g., sodium bicarbonate), which may be administered intravenously. Raising the urine pH to a basic level promotes cleavage of the ester in conjugates or catabolites thereof localized in the kidneys. Clearance of the released radionuclide metal chelates from the body is thereby enhanced. Administration of such agents to promote cleavage of ester linkers in vivo is described in U.S. Patent Application Serial No. 07/251,900, which is hereby incorporated by reference.

20

The comparatively low intestinal localization of the therapeutic radiolabeled polymeric carrier antibodies of the present invention or catabolites thereof permits increased dosages, since intestinal tissues are exposed to less radiation. The clarity and accuracy of diagnostic images also is improved by the reduced localization of radiolabeled polymeric carrier antibodies or catabolites thereof in normal tissues.

25

The above disclosure generally describes the present invention. A more complete understanding can be obtained by reference to the following specific examples which are

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provided for purposes of illustration only, and are not intended to limit the scope of the invention.

EXAMPLE 1

5 Three peptide carriers containing 6, 12, and 18 α -amino acids with different side chain hydroxyl groups are synthesized to show the use of hydrazones in covalently linking to agents. The requisite peptides are synthesized using the solid phase methodology of Merrifield (G. Barany and R.B; Merrifield, "The Peptides. Analysis, Synthesis and Biology" E. Gross and J. Meinhofer, Editors, Academic Press, New York, pages 1-284 (1980)).

15 This example first involves the synthesis of peptide 1, N-Acetyl-L-seryl-L-aspartyl(β -Otce)-L-seryl-L-threonyl-L-aspartyl-(β -Otce)-L-threonyl- γ -aminobutyric acid. This is followed by the oxidation of the hydroxyl amino acid side chain groups to carbonyl groups. These carbonyl groups are then condensed with the hydrazide groups on the agents. Next, there is formation of the active ester on the C-terminal of the peptide. This enables the peptide or polymeric carrier with attached agents to conjugate with the antibody. The general procedure for the synthesis of a polymeric carrier with attached agents and the conjugation of the polymeric carrier to an antibody is illustrated in Figure 1. Figure 2 illustrates a specific polymeric carrier synthesis and a specific conjugation procedure.

30 The above compounds are synthesized as C-terminal carboxylates using PAM resin attached to the first C-terminal amino acid (J.M. Stewart and J. Young, "Solid

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phase peptide synthesis", Pierce Chemical Company, Rockford, Illinois, 1984)) on an Applied Biosystems 430 A synthesizer using its specific protocols with N-methylpyrrolidone as a coupling solvent (User's manual: Model 430A synthesizer. Applied Biosystems, Inc., Foster City, CA)).

The preferred protecting groups are Ser (O-benzyl), Thr (O-benzyl), Glu(O-t-butyl), Glu(O-benzyl), Asp(O-t-butyl) and Tyr(Br-Cbz) (G. Barany and R.B. Merrifield, "The Peptides. Analysis, Synthesis and Biology" E. Gross and J. Meinhofer, Editors, Academic Press, New York, pages 1-284 (1980)). The other preferred protecting group for glutamic and aspartic acids (and other carboxyl bearing side chains) is the trichloroethyl ester trichloroethoxycarbonyl for tyrosine (Tce). The presence of this protecting group on the carboxyl of Asp and Glu residues offer protection through the sequence of derivatization of the side chain, attachment of the agents and the final activation of the terminal carboxyl group for conjugation to the targeting molecule. After the activation, the trichloroethyl group(s) can be removed by the using Zn-HOAc or Zn-THF-phosphate buffer (R.B. Woodward, K. Heusler, J. Gosteli, P. Naegeli, W. Oppolzer, R. Ramage, S. Ranganathan and H. Vorbruggen, J. Amer. Chem. Soc., 88, 852 (1989) and M.F. Sommelhack and G. E. Heinsohn, J. Amer. Chem Soc., 94, 5139 (1972)). After first deblocking by trifluoroacetic acid, the N-terminal residue is acetylated using acetic anhydride and finally cleaved from this resin using HF (See Figure 1).

The cleavage of peptides from the resin are accomplished using the low-high HF cleavage procedure of Tam and

- 35 -

Merrifield (J.P. Tam, W.F. Heath and R.B. Merrifield, "SN₂ deprotection of synthetic peptides with low concentration of HF in dimethyl sulfide: evidence and application in peptide synthesis." J. Amer. Chem. Soc., 105, 6442 (1983)) (method A) or in 10:1:1:2 (by volume) of HF:anisole:dimethylsulfide:p-thiocresol for 1 hour at 5° to 0°C. After cleavage, the organic scavengers are extracted from the resin 3 times with ether and the peptides extracted twice with 5 mL volume of 20-40% HOAc/H₂O. After lyophilization, the peptides are purified on a semi-preparative Vydec LC4 reversed phase column using a gradient of 100% H₂O-0.1% TFA to 40% H₂O-0.1% TFA+60% CH₃CN-0.1% TFA. They are analyzed for correct amino acid composition and molecular weight by FAB mass spectrometry (T.D. Lee, "Methods of Protein Micro-characterization" J.E. Shively, editor. The Humana Press, Clifton, New Jersey, p. 403 (1986).

It is necessary to prepare the corresponding C-14 labeled peptides at the N-terminal residue acetyl for the purpose of determining the stoichiometry of attachment of peptides and modified peptides containing therapeutic molecules. The N-terminal residue after the first deblocking of the N-terminal Boc group is acetylated using labeled acetic anhydride. As an example, 10 mg of the peptide is N-acetylated with C-14-acetic anhydride (1 mCi, 11.3 mCi/mmol) which is added and shaken for 2.5 hours with the resin. A 5-fold molar excess of diisopropylethylamine was added and N-acetylation was continued for 30 minutes. Peptide resin sealed in 1 inch square polypropylene bags was washed several times with 4 mL/bag of methylene chloride, 5% diisopropylethylamine/ methylene chloride and

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5 finally with 10% cold acetic anhydride/methylene chloride to complete the acetylation. Excess labelled anhydride was washed from the resin by consecutive rinses of methylene chloride, dimethyl formamide, isopropanol, methylene chloride, methanol and the resin was dried overnight prior to deblocking by the procedures described above.

10 To avoid the potential proteolytic degradation of the peptide or polymeric carrier attached to the targeting molecules while in the serum, the N-terminal residue or all the residues are in the D-configuration. The change in the configuration of the peptide backbone will not alter the rate of the release of the therapeutic molecules attached to the side chain. However, this change may
15 diminish the immunogenicity of the peptide backbone of these carriers.

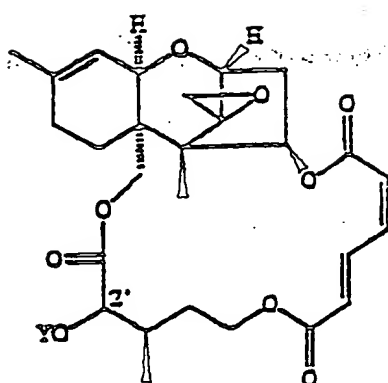
The next step involves Moffatt oxidation of peptide 1 to the corresponding carbonyl compound 2. The oxidation of
20 the peptide is carried out using DMSO, DCC, pyridine trifluoroacetate, and benzene or toluene. Moffatt oxidation is preferred for compound 2 since the procedure does not result in over oxidation of the hydroxyl compound. (For general methods see, A.F. Cook and J.G. Moffatt, J. Amer. Chem. Soc., 89, 2697 (1967) and K. E. Pfitzner and J.G. Moffatt, J. Amer. Chem Soc., 87, 5661
25 (1965)).

30 The next step is preparation (modification) of therapeutic molecules by changing their alcohol groups to hydrazides and then condensing them with modified peptides. The therapeutic molecules of interest are Verrucarin A and Roridin A which belong to the trichothecene group of

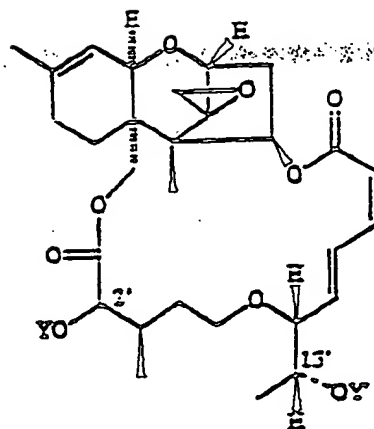
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antibiotics (B.B. Jarvis and A. Acierto in "Trichothecene
Mycotoxicosis: Pathophysiological Effects" Vol. 1. V. R.
Beasley, Editor, CRC Press, Boca Raton, FL, 1989. pp.
73-105). These compounds with broad spectrum biological
5 activities are the most potent synthesis inhibitors
containing C, H and O. They exert their inhibition by
interacting with the EF2 on the ribosomes (C.S.
McLaughlin, M.H. Vaughen, I.M. Campbell, I.M. Wei and B.S.
Hansen, "Mycotoxins in Human and Animal Health", J.V.
10 Rodericks, Editor. Pathotox Publishers, 1977, pp 263-
273). The structures of these compounds are shown below.
Verrucarin A (6) and Roridin A (8) were converted to the
corresponding succinyl hydrazide derivatives (7 from 6,9
and 10 from 8) according to published procedures (R. O.
15 Kollah, "The Chemistry and Biology of Macrocyclic
Trichothecenes", Ph.D. Thesis, University of Maryland,
1989; M. Zeng, "Studies in Chemical and Biological
Structures of Macrocyclic Trichothecenes", Ph.D. Thesis,
University of Maryland, 1989; V.M. Vrudhula, T.M.
20 Comezoglu and A. Srinivasan, Abstract No. MEDI 50, ACS
National Meeting, Boston, MA, April 1990).

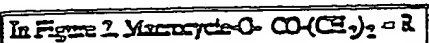
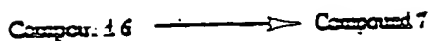
A similar strategy can be used to convert other molecules
of therapeutic interest containing alcohol function to
25 hydrazide (after incorporating a succinyl moiety) for
attachment to the defined polymer 2. In a similar manner,
molecules of therapeutic interest containing a carboxylic
acid function can be attached to the defined polymer via
the formation of a hydrazide.



Y = HVerrucaric A 6

Y = CO-(CH₂)₇-CONENE₂ 7
Verrucaric A-O-methylhydrazide

Y = Y = OH Roridin A 8

Y = CO-(CH₂)₇-CONENE₂; R = H 9
(Roridin A-O-methylhydrazide)Y = E; Y = CO-(CH₂)₇-CONENE₂ 10
(Roridin A-O-methylhydrazide)

- 20 The next procedure is preparation of hydrazone 3 from compound 2 and Verrucaric A hydrazide 7. To a solution of the peptide (1 mmol) in isopropanol 5 mmol of Verrucaric A hydrazide (7; 10 mmol) is added and the solution is allowed to stand at room temperatures for several hours.
- 25 The formation of hydrazone is followed chromatographically and is isolated either by crystallization or by C-18 column chromatography. The product is characterized by NMR and FAB mass spectrometry.
- 30 The hydrazone derived from peptide 4 and Roridin A derivatives 9 and 10 are prepared in a similar manner.

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The next synthesis is the preparation of active ester 4 of peptide 3 (See Figure 3). To a solution of the peptide 3 in DMF, from the above reaction, 3 equivalents of 2,3,5,6-tetrafluorophenol and 3 equivalents of DCC are added and the solution is stirred at room temperature for 10-12 hours. The precipitated dicyclohexylurea is removed by filtration and the residue is chromatographed to isolate the product.

The product is dissolved in a phosphate buffer containing 10% tetrahydrofuran and the trichloroethyl groups are removed according to the procedure of M.F. Sommelhack and G.E. Heinsohn (J. Amer. Chem. Soc., 94 5139 (1972)) to yield the peptide or polymeric carrier 4, containing the therapeutic molecules and an active ester for attachment to the targeting molecule.

The last step is the conjugation of the active ester 4 to the NR-LU-10 to give the conjugate 5. The active ester is condensed with NR-LU-10 murine monoclonal antibody, which recognizes a pancarcinoma antigen. Other proteins or fragments may be substituted for the NR-LU-10 antibody. To a solution of the antibody at pH 9-9.5, a solution of the active ester in 250 mM bicarbonate buffer at pH 9.3 is added and gently agitated to mix and incubated at room temperature for 30 minutes to allow conjugation of the peptide carrier to the antibody. The conjugate is purified in a column containing an anion exchanger DEAE-sephadex or QAE-sephadex. All of the above reactions are shown in Figure 2.

In a similar manner, conjugates are prepared from longer chain peptides, N-Acetyl-[L-seryl-L-aspartyl(β -Otce)-L-

- 40 -

seryl-L-threonyl-L-aspartyl-(β -Otce)-L-threonyl]₂- γ -aminobutyric acid, peptide 11 and N-Acetyl-L-seryl-L-aspartyl(β -Otce)-L-seryl-L-threonyl-L-aspartyl β -Otce)L-threonyl- γ -aminobutyric acid, peptide 12.

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General procedure for the evaluation of stability of hydrazones follows. Prior to the evaluation of conjugates the hydrazones derived from peptides 1, 11, and 12 are converted to the free acids 13-15 (see Figure 3). For the experiments in human serum stability, the hydrazone under investigation is incubated in fresh human serum at 37°C at a concentration of 1 mg/mL. Aliquots (100 μ L) at different time points (2-150 hours) are diluted with equal volumes of acetonitrile. The suspension is centrifuged and the centrifugate is analyzed by HPLC for the presence of the therapeutic drug released. In a similar manner, the compounds are tested for their stability at pH 5.6.



EXAMPLE 2

5 This example covers the attachment of bifunctional chelate ligands to the defined peptide or polymeric conjugation of the carrier to the antibody followed by radiolabeling .

10 The procedures in this example are the synthesis of N-Acetyl-L-tyrosyl (O-CO-CH₂-CCl₃)-L-Asp(β -OtBu)-Glu(γ -OtBu)Gly-Glu(γ -OtBu)- γ -Aba-PAM resin 16, the removal of protecting groups from the carboxyl groups in Asp and glutamyl residues using trifluoroacetic acid to synthesize, peptide 17, the condensation of bifunctional chelate, S-ethoxyethylmercapto-acetylglycylglycylserine-trichloroethyl ester 24 to give 25, the cleavage of this peptide from the resin to give 26, the activation of the terminal carboxylic acid to give 27, the deprotection (to 28), and the radiolabeling to give the chelate 29, followed by conjugation to the antibody to yield the conjugate 30 (see Figure 4).

20 The requisite peptide, N-Acetyl-L-tyrosyl (O-CO-CH₂-CCl₃) - L-Asp(β -OtBu)-Glu(γ -OtBu)-Gly-Glu(γ -OtBu)- γ -Aba-PAM resin 16, is synthesized using solid phase methodology of Merrifield (G. Barany and R. B. Merrifield, "The Peptides. Analysis, Synthesis and Biology". E. Gross and J. Meinhofer, Editors, Academic Press, New York, pages 1-284 (1980)). The protecting group in each step is 9-flourenylmethoxycarbonyl (Fmoc) rather than the N-tBoc group used in the synthesis of 1. This methodology
25 conserves the protecting group of the Glu and Asp (and other amino acid residues bearing a carboxyl side chain). Removal of the Fmoc protecting group in each successive
30

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step is accomplished by using aqueous piperidine. Acetylation is accomplished according to the procedure described earlier.

- 5 Preparation of C-14 labeled peptides at the N-terminal residue acetyl. It is necessary to prepare the corresponding C-14 labeled peptides for the purpose of determining the stoichiometry of attachment of peptides and modified peptides containing therapeutic molecules.
- 10 The N-terminal residue after the first deblocking of the N-terminal Fmoc group is acetylated using labeled acetic anhydride. As an example, 10 mg of the peptide is N-acetylated with C-14 acetic anhydride (1 mCi, 11.3 mCi/mmol) which is added and shaken for 2.5 hours with the
- 15 resin. A 5-fold molar excess of diisopropylethylamine is added and N-acetylation was continued for 30 minutes. Peptide resin sealed in 1 inch square polypropylene bags was washed several times with 4 mL/bag of methylene chloride, 5% diisopropylethylamine/methylene chloride and
- 20 finally with 10% cold acetic anhydride/methylene chloride to complete the acetylation. Excess labelled anhydride is washed from the resin by consecutive rinses of methylene chloride, dimethyl formamide, isopropanol, methylene chloride, methanol and the resin was dried overnight prior
- 25 to removal of the t-Boc protecting groups.

- To avoid the potential proteolytic degradation of the peptide carrier attached to the biological macromolecules while in the serum, the N-terminal residue or all the
- 30 residues are in the D-configuration. The change in the configuration of the peptide back bone will not alter the rate of the release of the therapeutic molecules attached

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to the side chain. This change may also diminish the immunogenicity of the peptide backbone of these carriers.

5 The synthesis of N-Acetyl-L-Tyr-L-Asp-Glu-Gly-Glu- γ -Aba
PAM resin 17. The peptide still attached to the resin is
deblocked using trifluoroacetic acid (conversion of tbutyl
esters of glu and asp residues) to -COOH according to the
general procedure (G. Barany and R.B. Merrifield, "The
10 Peptides. Analysis, Synthesis and Biology" E. Gross and J.
Meinhofer, Editors, Academic Press, New York, pages 1-284
(1980)).

15 The synthesis of S-ethoxyethylmercaptoacetyl-
glycylglycylserinetrichloroethyl ester 24 (see Figure 5)
involves first the synthesis of N-t-Boc-Serine-O-benzyl-
trichloroethyl ester 18. To a solution of N-t-Boc-
serine-O-benzyl ether (5 mmol) in methylene chloride
containing 5 mmol of triethylamine, 5 mmol of N,
20 N-dicyclohexylcarbodiimide was added and the solution was
stirred at room temperature overnight. The precipitated
dicyclohexylurea was filtered and the filtrate was washed
with 1% HCl and water. The organic layer was dried over
anhydrous Na₂SO₄, and evaporated to give the trichloroethyl
ester, which was purified over a silica gel column.

25 Serine trichloroethyl ester trifluoroacetate 19 is
prepared in the following manner. A solution of 4 mmol of
the above compound 18, in 50 mL of glacial acetic acid
containing 200 mg of palladium on charcoal was
30 hydrogenated at 60 psi in a Paar apparatus for 10-12
hours. The catalyst was removed by filtration over celite
and the solvent was removed in vacuo to give N-t-Boc

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serine trichloroethyl ester, an oil, which was dried overnight and used without further purification. The oil was stirred with 10 mL 50% trifluoroacetic acid-CH₂Cl₂ for 3 hours at room temperature to remove the Boc group. The mixture was evaporated to dryness, coevaporated several times with methylene chloride and dried to give 19. The compound was homogeneous by TLC and was used in the next step without further purification.

10 S-(1-ethoxyethyl) mercaptoacetic acid 20 is prepared according to the following. A solution of mercaptoacetic acid (17.4 mL, 250 mmol) in 125 mL of dichloromethane containing p-toluenesulfonic acid monohydrate (0.24 g, 1.26 mmol) was cooled to -18 to -25°C with stirring. Ethyl vinyl ether (23.9 mL, 250 mmol) in 125 mL of dichloromethane was added dropwise to the cold solution over a period of 90 minutes. The stirring was continued for an additional 30 minutes with the temperature maintained in the -18 to -25°C range. Then 200 mL of pH7 phosphate buffer was added, and the reaction mixture was allowed to warm with stirring for 10 to 15 minutes. The mixture was then poured into a flask containing 900 mL of ethyl acetate and 200 mL of water. Layers were separated and the aqueous portion extracted twice with ethyl acetate. The organic layers were combined, washed with brine and dried (MgSO₄). Removal of the solvent left 31.4 g of S-(1-ethoxyethyl) mercaptoacetic acid 20 as a colorless oil (77% yield): ¹H NMR (CDCl₃) 1.15 (t, J=7.0Hz, 3H), 1.52 (d, J=6.4Hz, 3H), 3.36 (s, 2H), 3.60 (m, 2H), 4.84 (q, J=6.4Hz, 1H), 11.65 (s, 1H). The material was used without further purification.

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Succinimidyl S-(1-ethoxyethyl) mercaptoacetate **21** is prepared according to the following procedure. A solution of S-(1-ethoxyethyl) mercaptoacetic acid (5.76 g, 35.1 mmol) and N-hydroxysuccinimide (4.85 g, 42.1 mmol) was prepared in 100 mL of anhydrous THF. To this was added a solution of 1,3-dicyclohexylcarbodiimide (8.70 g, 42.1 mmol) in 65 mL of anhydrous THF. The mixture was stirred at room temperature for 2 hours or until TLC analysis indicated complete formation of the succinimidyl ester. The mixture was then filtered, and the filtrate was concentrated in vacuo to a viscous residue. The residue was dissolved in ethyl acetate, washed with water, brine, and dried (MgSO_4). Removal of the solvent left the crude succinimidyl ester as an oil, which was further purified by flash chromatography on silica gel, using ethyl acetate-hexanes as the column eluent, to give 5.1 g of S-(1-ethoxyethyl) mercaptoacetic acid succinimidyl ester as a colorless oil (56% yield): ^1H NMR (CDCl_3) 1.21 (t, $J=7.0\text{Hz}$, 3H), 1.58 (d, $J=6.4\text{Hz}$, 3H), 2.83 (s, 4H), 3.60 (m, 4H), 4.88 (q, $J=6.4\text{Hz}$, 1H).

The synthesis of **22** is as follows. Solid NaHCO_3 (1.09 g, 13.0 mmol) was added to a solution of glycylglycine (1.22 g, 9.3 mmol) in 10 mL of water. After gas evolution ceased, a solution of (2.66 g, 10.2 mmol) in 12 mL of CH_3CN was added to the reaction mixture. The mixture was stirred at room temperature for 22 h, then evaporated in vacuo. The residue was purified by flash chromatography on silica gel (85:10:5 $\text{CH}_3\text{CN}:\text{H}_2\text{O}:\text{HOAc}$) to yield 2.2 g (86%) of **22** as a viscous oil. ^1H NMR (DMSO) 8.26 (t, 1H), 8.08 (t, 1H), 4.80 (q, 1H), 3.73 (m, 4H), 3.52 (m, 2H), 3.24 (s, 2H), 1.43 (d, 3H), 1.10 (t, 3H).

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The following are details on the synthesis of 23. 1,3 Dicyclohexylcarbodiimide (0.66 g, 3.2 mmol) was added to a stirring solution of 22 (0.81 g, 2.9 mmol) and N-hydroxysuccinimide (0.37 g, 3.2 mmol) in 10 mL of CH₃CN. After stirring for 2 h, the mixture was filtered and the filtrate was evaporated in vacuo. The residue was purified by flash chromatography on silica gel (96:4 EtOAc:HOAc) to yield 0.80 g (73%) of 23 as a viscous oil. ¹H NMR (DMSO) 8.54 (t, 1H), 8.29 (t, 1H), 4.80 (q, 1H), 4.27 (d, 2H), 3.78 (d, 2H), 3.53 (m, 2H), 3.24 (s, 2H), 2.81 (s, 4H), 1.43 (d, 3H), 1.09 (t, 3H).

The synthesis of S-ethoxyethylmercaptoacetyl glyceryl glycerylserinetrichloroethyl ester 24 is prepared in the following manner (see Figure 5). Triethyl-amine (2 mmol) was added to a solution of 19 (1.7 mmol) and 23 (1.7 mmol) in 5 mL of anhydrous dimethylformamide. After stirring for 2.5 hours at room temperature the mixture was evaporated in vacuo. The resulting residue was taken up in ethyl acetate (20 mL) and washed with water, saturated sodium chloride and dried over sodium sulfate, filtered and evaporated. The residue was purified over a C-18 column to give pure 24, which was used in the condensation.

The condensation of 24 with the -COOH residues of Glu and Asp in 17 occurs in the following manner. Solid cleavage of peptides from the resin is accomplished using the low-high HF cleavage procedure of Tam and Merrifield (J.P. Tam, W.F. Heath and R.B. Merrifield, "SN₂ deprotection of synthetic peptides with low concentration of HJ in dimethyl sulfide: evidence and application in peptide

synthesis." J. Amer. Chem. Soc., 105, 6442 (1983)) (Method

A) or in 10:1:1:2 (by volume) of HF:anisole:

dimethylsulfide:p-thiocresol for 1 hour at 5°-0°C. After

cleavage, the organic scavengers are extracted from the

resin 3 times with ether and the peptides extracted twice

with 5 mL volume of 20-40% HOAc/H₂O. After

lyophilization, the peptides are purified on a

semi-preparative Vydec LC4 reversed phase column using a

gradient of 100% H₂O-0.1% TFA to 40% H₂O-0.1% TFA+60%

CH₃CN-0.1% TFA. They are analyzed for correct amino acid

composition and molecular weight by FAB mass spectrometry

(Ref: T.D. Lee, "Methods of Protein Microcharacterization"

J.E. Shively, editor. The Humana Press, Clifton, New

Jersey, p. 403 (1986)).

The following is the preparation of the active ester 27 of

26. To a solution of the peptide 26 in DMF, from the above

reaction, 3 equivalents of 2,3,5,6tetrafluorophenol and 3

equivalents of DCC are added and the solution is stirred

at room temperature for 10-12 hours. The precipitated

dicyclohexylurea is removed by -filtration and the residue

is chromatographed to isolate the product, 27.

The product 27 is dissolved in a phosphate buffer

containing 10% tetrahydrofuran and the trichloroethyl

groups are removed according to the procedure of M. F.

Sommelhack and G.E. Heinsohn (J. Amer. Chem Soc., 94, 5139

filtration and the residue is chromatographed to isolate

the product, 27.

The product 27 is dissolved in a phosphate buffer

containing 10% tetrahydrofuran and the trichloroethyl

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groups are removed according to the procedure of M. F. Sommelhack and G.E. Heinsohn (J. Amer. Chem Soc., 94, 5139 (1972)) to yield the peptide carrier 28, containing the chelator capable of forming metabolically stable complexes with radionuclides and an active ester for attachment to the targeting molecule.

The following is the radiolabeling procedure with ^{186}Re . The peptide containing the chelator radiolabeled with ^{186}Re according to the following procedure. Sodium perrhenate produced from a W/Re generator is combined with citric acid (a preferred complexing agent for ^{186}Re), a reducing agent (usually SnCl_2). The resulting ^{186}Re -citrate exchange complex is heated with the chelating compound 28 at $75^\circ\text{--}100^\circ\text{C}$ for 10-15 minutes and then transferred to a 0°C ice bath for a few minutes to obtain the peptide 29 containing ^{186}Re -complexes on the side chain.

The above solution containing the chelate is removed from the ice bath, 2.0 mL of 250 mM sodium bicarbonate buffer (pH 9-10) is added and the vial is agitated to mix. Immediately, the antibody (whole or fragments) is added and incubated at room temperature for 10-15 minutes to complete the conjugation to the antibody. The conjugate so produced is purified using an anion exchange column (DEAE-sephadex or QAE-sephadex) prepared under aseptic conditions to yield 30.

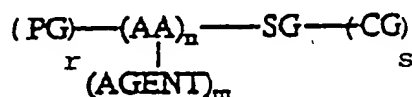
In a similar approach, peptides 31 and 32 are synthesized by solid phase procedure and the antibody conjugates 37 and 38 prepared. The intermediates in the case of these oligomer syntheses are shown in Figure 6.

The invention now being fully described, it will be apparent to one of ordinary skill in the art that many changes and modifications can be made without departing from the spirit or scope of the invention.



CLAIMS

1. A chemically defined polymeric carrier comprising a series of α -amino acids in any combination containing side chains to which agents covalently join through cleavable linkers either directly or covalently join through cleavable linkers after chemical modification of the side chains and represented by the formula:

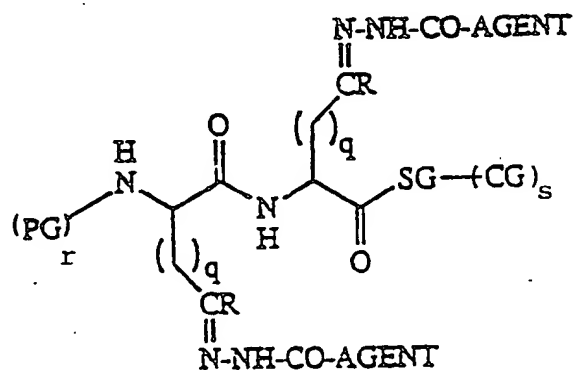


wherein PG is an N-terminal protecting group;
AA is an α -amino acid;
SG is a spacer group that by preventing steric
hindrance by agents appended from the C-
terminal end of the carrier promotes efficient
attachment of the polymeric targeting molecule;
CG is a conjugation group useful for the
attachment of the polymer carrier to a
targeting molecule;
AGENT is a diagnostic or therapeutic agent, or
a chelating agent capable of binding diagnostic
or therapeutic radionuclides;
n is from 2 to about 18;
m is from 2 to about 18;
r is 0 or 1; and
s is 0 or 1.

2. The polymeric carrier of claim 1, further comprising
at least one α -amino acid with a side chain to which
an agent does not covalently join that functions as
a spacer to minimize interaction between the agents
covalently joined to the polymeric carrier.
3. The polymeric carrier of claim 1, further comprising
at least one α -amino acid with a charged or
hydrophilic side chain to which an agent does not
covalently join that provides increased solubility
to the polymeric carrier.
4. The polymeric carrier of claim 3, wherein the
 α -amino acid with a charged or hydrophilic side
chains is selected from the group consisting of
serine, threonine, lysine, arginine, histidine,
cysteine, aspartic acid, glutamic acid, asparagine,
glutamine, tyrosine, and tyrosine-O-SO₃.
5. The polymeric carrier of claim 1, wherein the N-
terminal protecting group, PG, is selected from the
group consisting of acetyl, propionyl, phenacyl-
sulfonyl, and substituted phenacylsulfonyl.
6. The polymeric carrier of claim 1, wherein the spacer
group, SG, is selected from the group consisting of
aminocaproic acid, aminopentanoic acid, γ -amino-
butyric acid, β -alanine, and glycine.
7. The polymeric carrier of claim 1, wherein the
conjugation group, CG, is selected from the group
consisting of active esters, isothiocyanates,

amines, hydrazines, maleimides or other Michael-type acceptors, thiols, and activated halides.

8. The polymeric carrier of claim 1, wherein the α -amino acids are all in the L configuration.
9. The polymeric carrier of claim 1, wherein the α -amino acids are all in the D configuration.
10. The polymeric carrier of claim 1, wherein the α -amino acids are any combination of L and D configuration.
11. The polymeric carrier of claim 1, wherein the α -amino acid, AA, is covalently joined through a hydrazone linkage to an agent and represented by the formula:



wherein PG is an N-terminal protecting group;
SG is a spacer group that by preventing steric hindrance by agents appended from the C-terminal end of the carrier promotes

efficient attachment of the polymeric carrier to a targeting molecule;
CG is a conjugation group useful for the attachment of the polymeric carrier to a

AGENT is a diagnostic or therapeutic agent, or a chelating agent capable of binding diagnostic or therapeutic radionuclides;

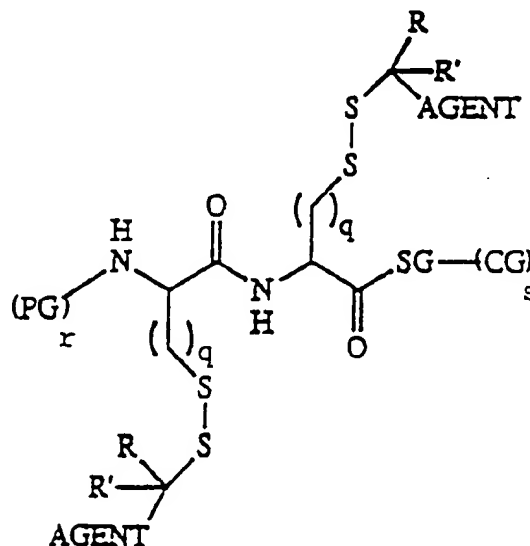
R is H, CH₃, phenyl, or phenyl substituted with electron-donating and/or electron-withdrawing groups;

q is 0 or 1;

r is 0 or 1; and

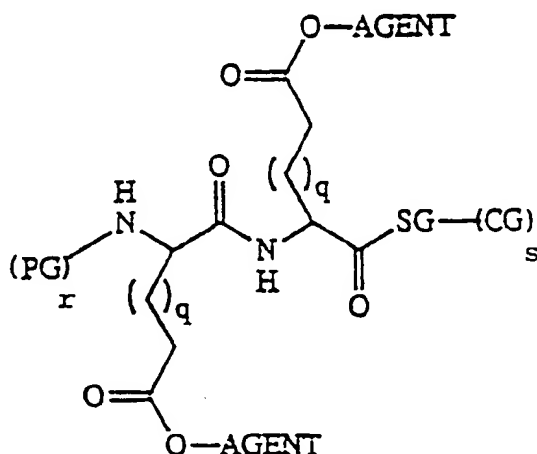
s is 0 or 1.

12. The polymeric carrier of claim 1, wherein the α -amino acid, AA, is covalently joined through a disulfide linkage to an agent and represented by the formula:



- 5 wherein PG is an N-terminal protecting group;
 SG is a spacer group that by preventing
 steric hindrance by agents appended from
 the C-terminal end of the carrier promotes
 efficient attachment of the polymeric
 10 carrier to a targeting molecule;
 CG is a conjugation group useful for the
 attachment of the polymeric carrier to a
 targeting molecule;
 AGENT is a diagnostic or therapeutic
 15 agent, or a chelating agent capable of
 binding diagnostic or therapeutic
 radionuclides.
 R is H or CH₃;
 R' is H or CH₃;
 20 q is 1 or 2;
 r is 0 or 1; and
 s is 0 or 1.

13. The polymeric carrier of claim 1, wherein the
 α-amino acid, AA, is covalently joined through an
 25 ester linkage to an agent and represented by the
 formula:

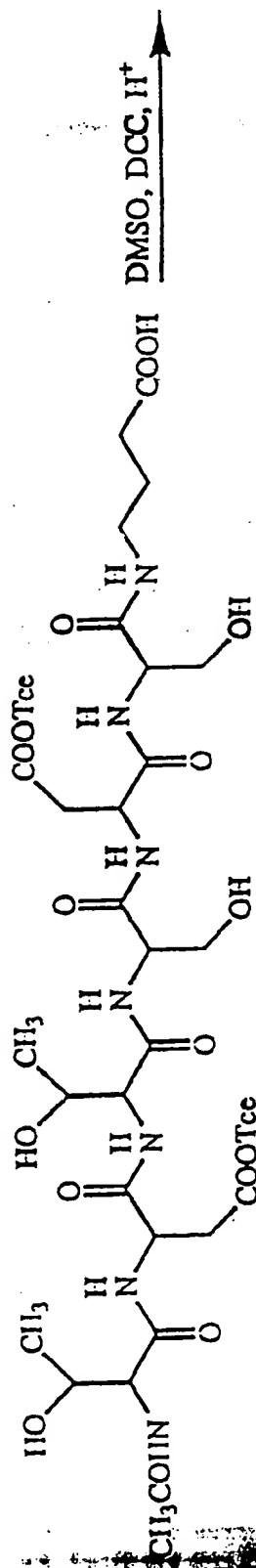


- 55 -

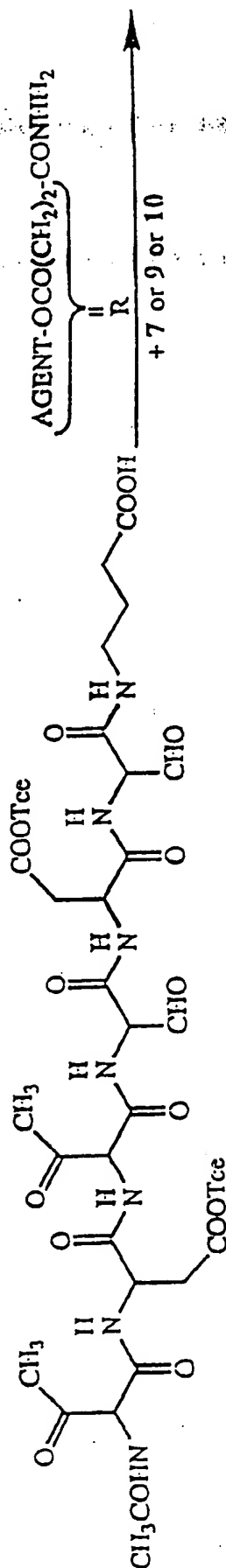
5 wherein PG is an N-terminal protecting group;
 SG is a spacer group that by preventing
 steric hindrance by agents appended from
 the C-terminal end of the carrier promotes
10 efficient attachment of the polymeric
 carrier to a targeting molecule;
 CG is a conjugation group useful for the
 attachment of the polymeric carrier to a
 targeting molecule;
15 AGENT is a diagnostic or therapeutic
 agent, or a chelating agent capable of
 binding diagnostic or therapeutic
 radionuclides;
 q is 0 or 1;
 r is 0 or 1; and
20 s is 0 or 1.

14. The polymeric carrier of claim 1, wherein the
 α -amino acids are covalently joined to agents
 through hydrazone linkages, disulfide linkages,
25 ester linkages, and any combinations thereof.

Figure 2

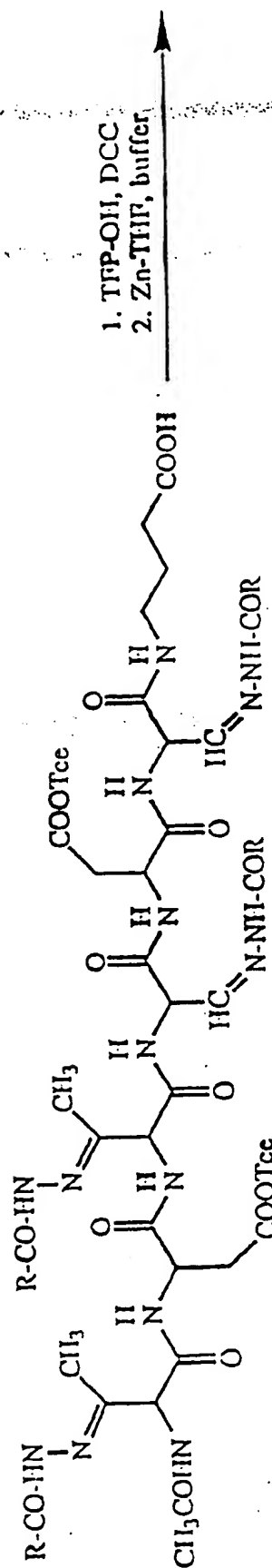
Ac-Thr-Asp(β -COOTce)-Thr-Ser-Asp(β -COOTce)-Ser-Aba-OHDMSO, DCC, H^+

1

AGENT-OCO(CH₂)₂-CONHCH₂

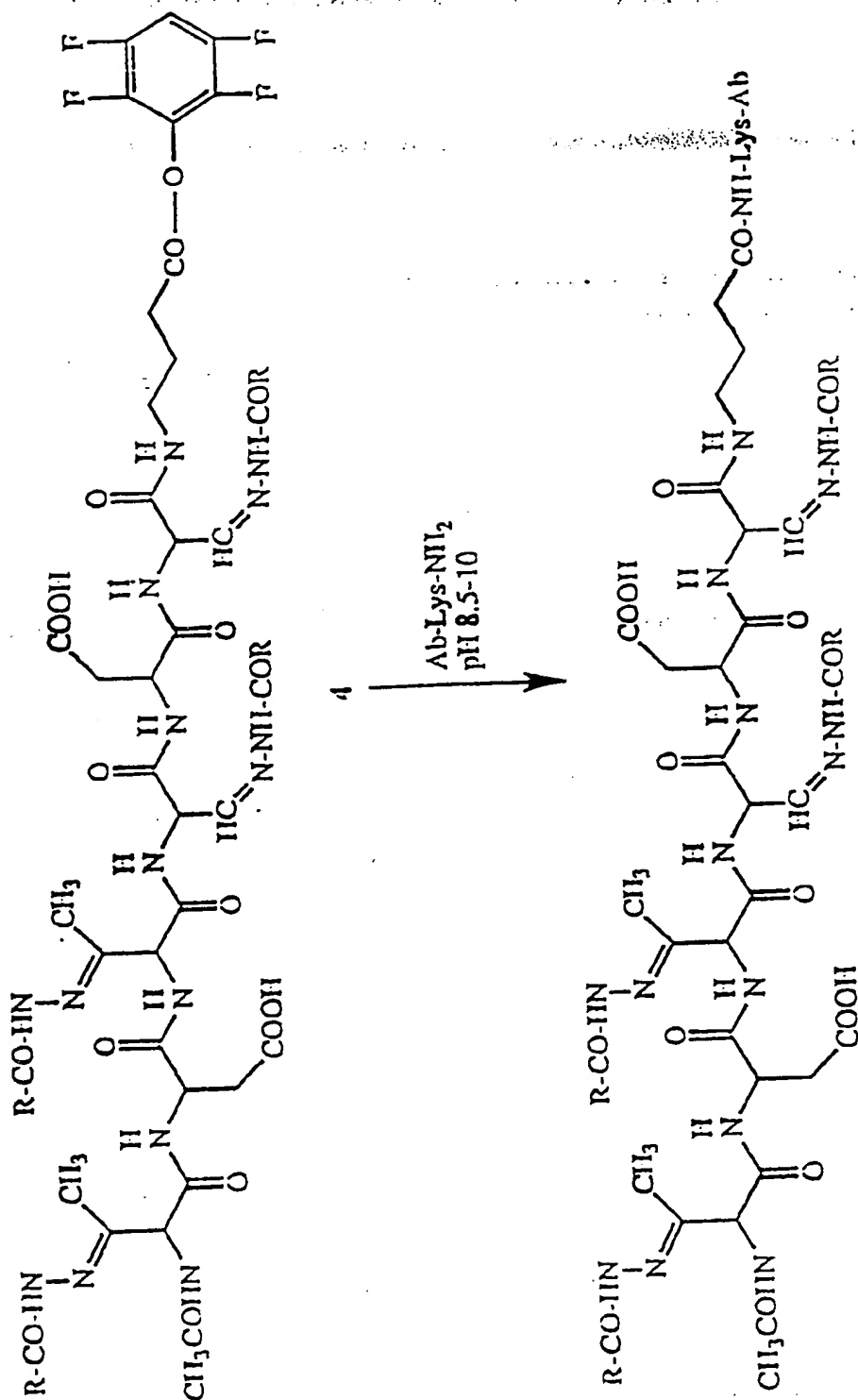
+ 7 or 9 or 10

2

1. TFP-OH, DCC
2. Zn-THP, bufferR = AGENT-OCO(CH₂)₂-

TFP-OH = 2,3,5,6-tetrafluorophenol

Figure 2(contd.)



Structure of the conjugate containing therapeutic drug attached to the defined peptide carrier attached to the antibody.

Figure 3

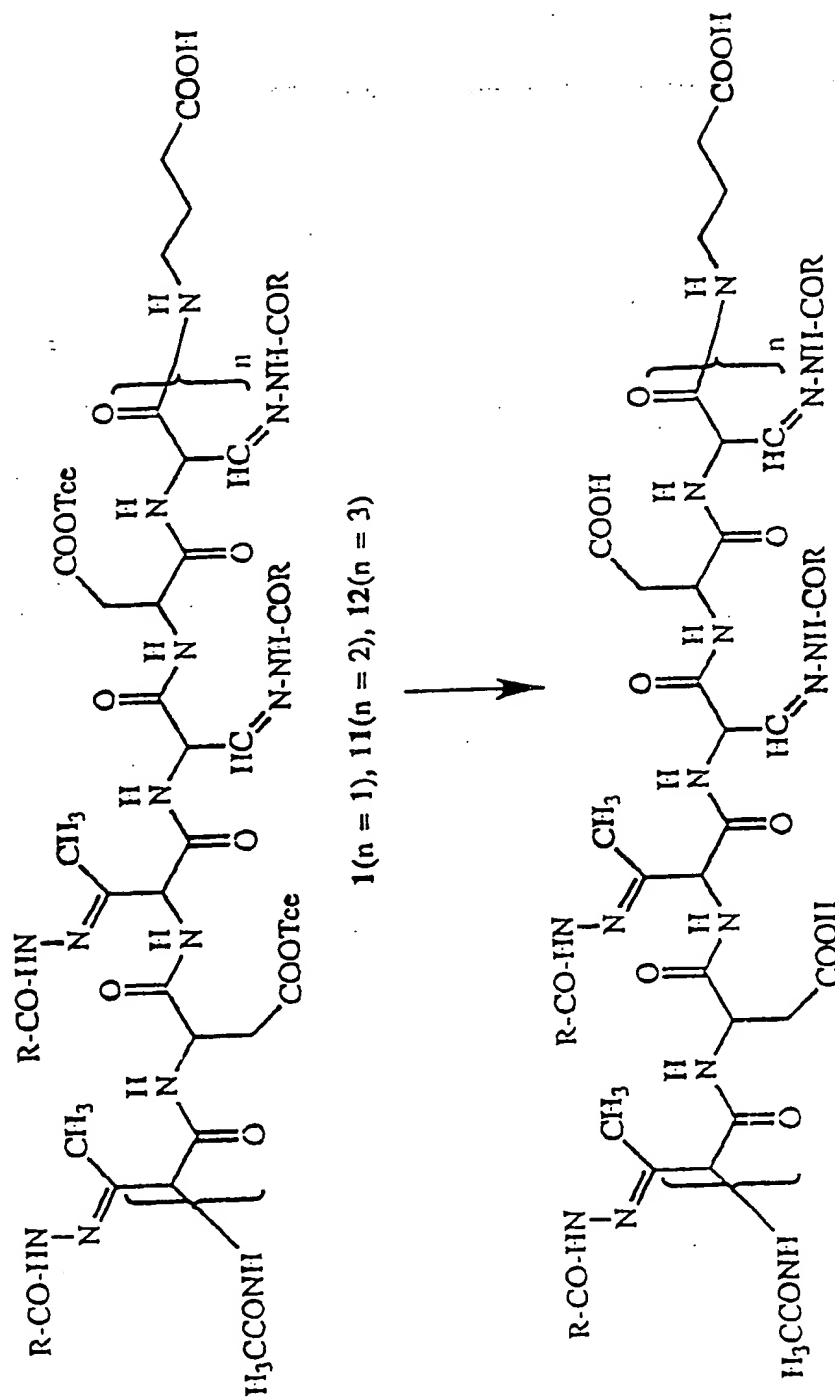


Figure 4

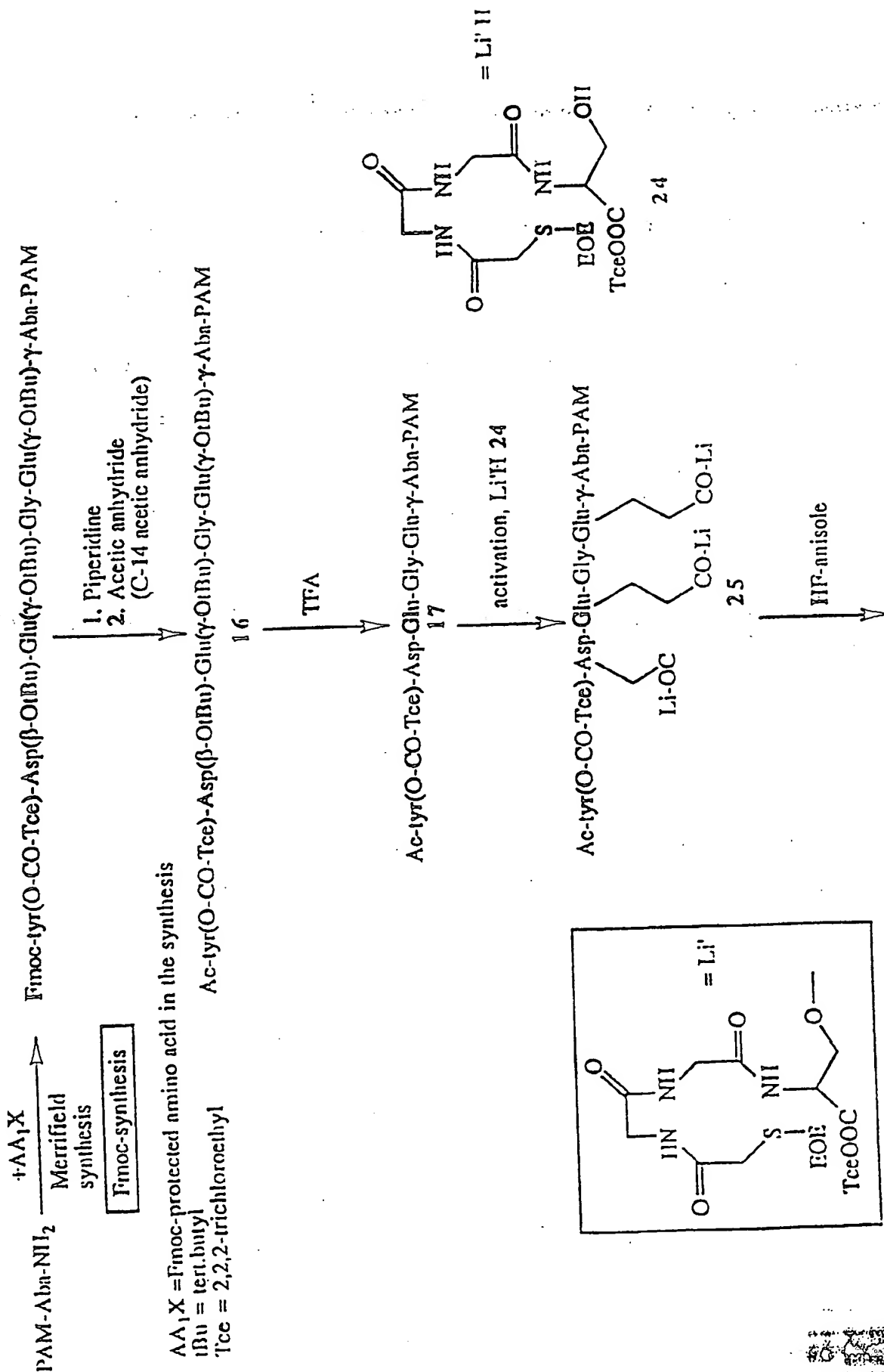


Figure 4 (contd.)

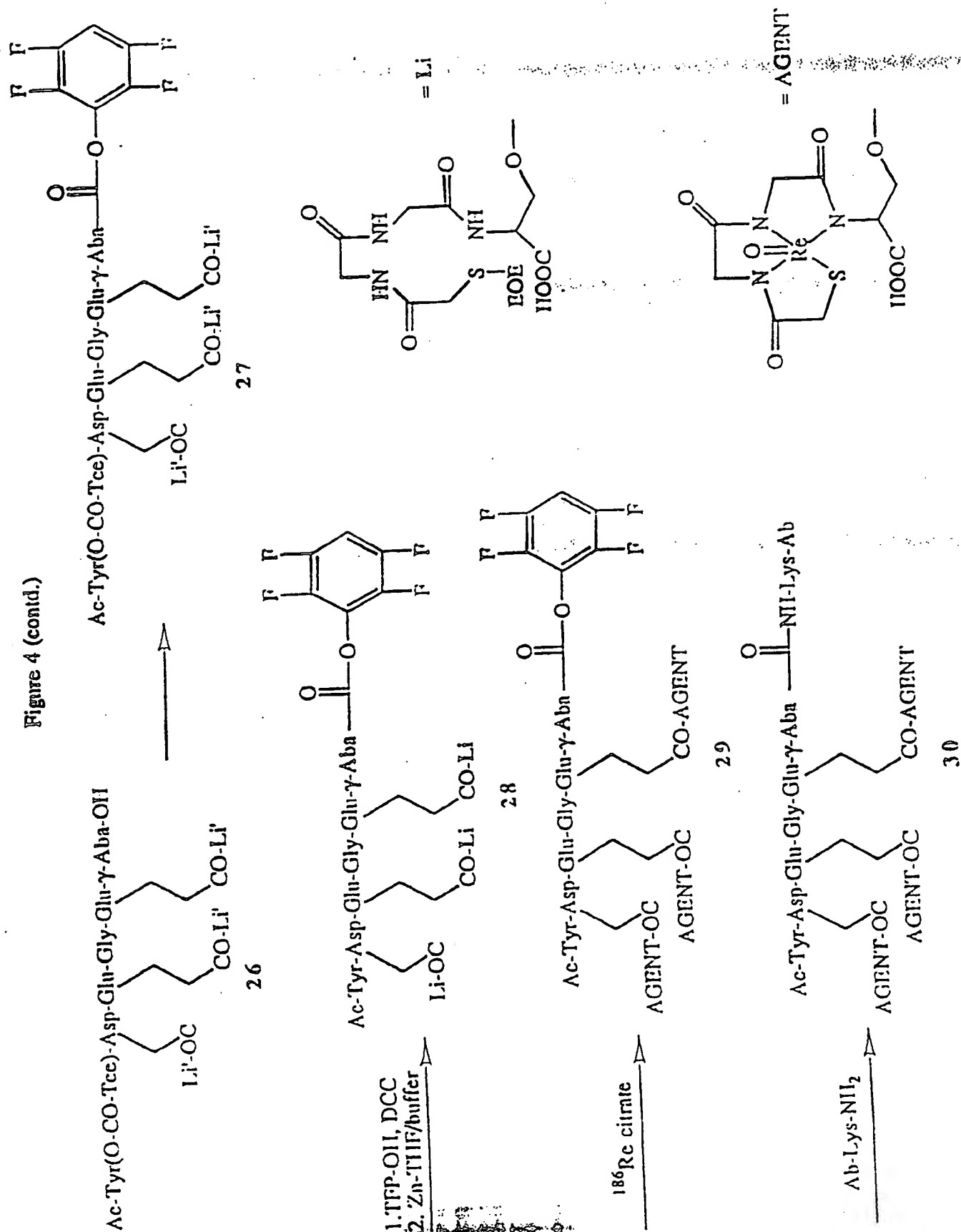
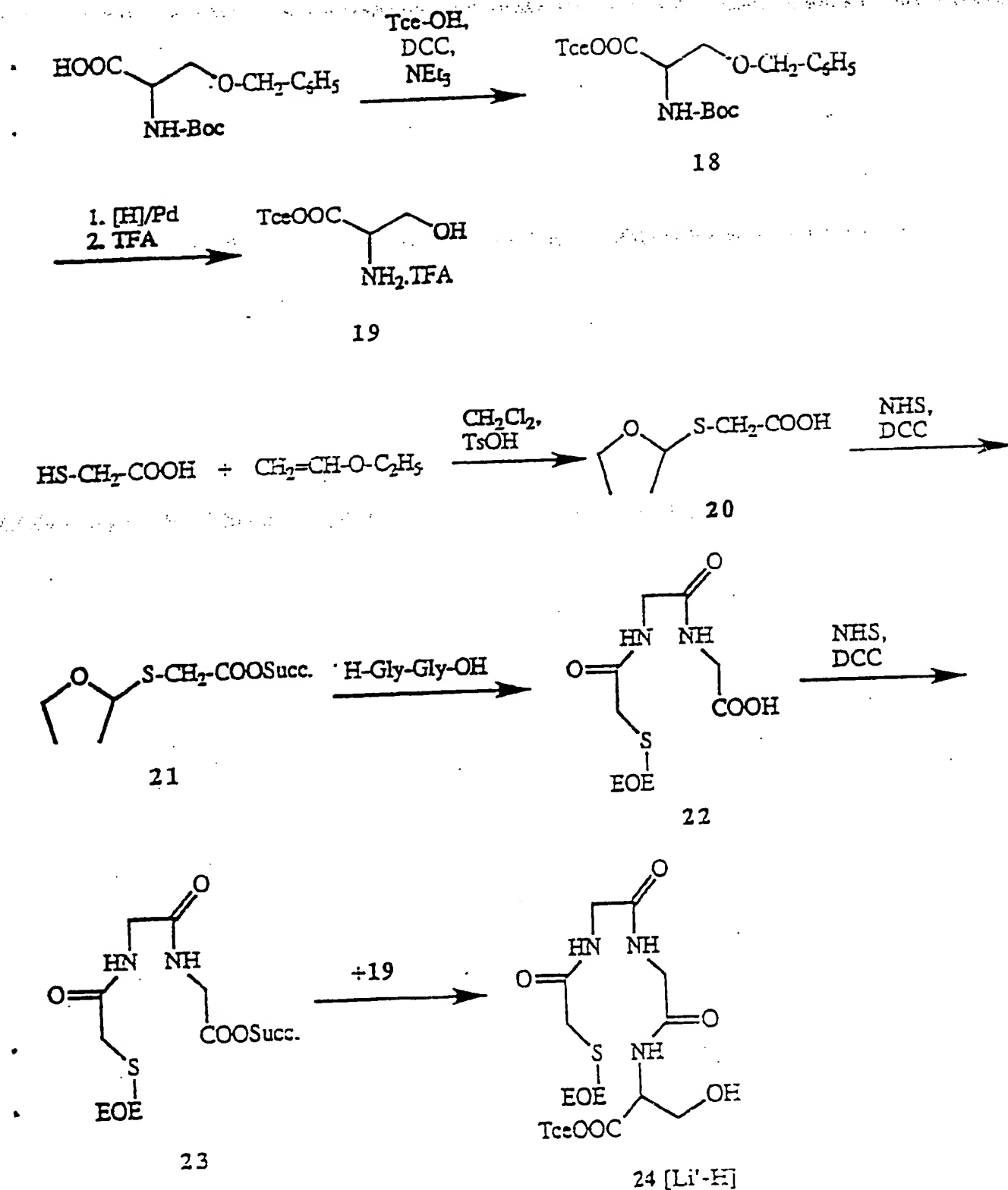


Figure 5



INTERNATIONAL SEARCH REPORT

International Application No. PCT/US91/07143

I. CLASSIFICATION OF SUBJECT MATTER (if several classification symbols apply, indicate all) *

According to International Patent Classification (IPC) or to both National Classification and IPC
 IPC (5): A61K 39/44, 43/00, 48/00, 49/02; C07K 15/28

II. FIELDS SEARCHED

Minimum Documentation Searched ⁷

Classification System	Classification Symbols
U.S.	530/345/389,402,807; 930/25,30,280; 424/1.1,9,85.91

Documentation Searched other than Minimum Documentation
 to the extent that such Documents are included in the Fields Searched *

III. DOCUMENTS CONSIDERED TO BE RELEVANT *		
Category *	Citation of Document, ¹¹ with indication, where appropriate, of the relevant passages ¹²	Relevant to Claim No. ¹³
X Y	US, A, 4,587,046 (GOODMAN ET AL.) 06 May 1986 See col. 6, line 67 - column 9, line 3, and column 11, line 48 - column 14 line 30.	1-7,10,13,14 1-14
Y	US, A, 4,543,211 (KATO ET AL.) 24 September 1985 See column 3, line 64 - column 4, line 26; column 13, lines 25-46; and column 17-19.	1,7,10,14
Y	US, A, 4,485,093 (RUNGE) 27 November 1984 See column 2, line 60 - column 3, line 4; column 4, lines 28 - 40; and column 4, line 62 - column 5, line 66.	1,7,10
Y	US, A, 4,867,973 (GOERS ET AL.) 19 September 1989 See column 7, lines 9-15 and 35-40; column 9, lines 17-38; column 13, lines 1-10; column 22, lines 37-62; and column 23, lines 52 - column 24, line 17.	1-14
P,Y	US, A, 4,997,913 (HELLSTROM ET AL.) 05 March 1991 See column 7, line 60 - column 8, line 59; Example 5, column 15 and 16; and column 18, lines 30-38.	1-5,7-10, 12, 14

- * Special categories of cited documents: ¹⁰
- "A" document defining the general state of the art which is not considered to be of particular relevance
 - "E" earlier document but published on or after the international filing date
 - "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
 - "O" document referring to an oral disclosure, use, exhibition or other means
 - "P" document published prior to the international filing date but later than the priority date claimed

- "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
- "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step
- "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
- "d" document member of the same patent family

IV. CERTIFICATION

Date of the Actual Completion of the International Search

03 January 1992

International Searching Authority

ISA/US

Date of Mailing of this International Search Report

07 FEB 1992

Signature of Authorized Officer

John M. Covert

FURTHER INFORMATION CONTINUED FROM THE SECOND SHEET

A US, A, 4,732,974 (NICOLOTTI ET AL.) 22 March 1988 1,7,10,13,14
See entire document.

Y WO, A, 87/05031 (CENTER FOR MOLECULAR MEDICINE AND
IMMUNOLOGY) 27 August 1987. See page 5, paragraphs
2 and 3, and page 8, paragraphs 1-3.

V. ☐ OBSERVATIONS WHERE CERTAIN CLAIMS WERE FOUND UNSEARCHABLE¹

This international search report has not been established in respect of certain claims under Article 17(2) (a) for the following reasons:

1. ☐ Claim numbers _____, because they relate to subject matter ¹² not required to be searched by this Authority, namely:

2. ☐ Claim numbers _____, because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out ¹³, specifically:

3. ☐ Claim numbers _____, because they are dependent claims not drafted in accordance with the second and third sentences of PCT Rule 6.4(a).

VI. ☐ OBSERVATIONS WHERE UNITY OF INVENTION IS LACKING²

This International Searching Authority found multiple inventions in this international application as follows:

1. ☐ As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims of the international application.

2. ☐ As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims of the international application for which fees were paid, specifically claims:

3. ☐ No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims; it is covered by claim numbers:

4. ☐ As all searchable claims could be searched without effort justifying an additional fee, the International Searching Authority did not invite payment of any additional fee.

Remark on Protest

- ☐ The additional search fees were accompanied by applicant's protest.
☐ No protest accompanied the payment of additional search fees.